



Short title: Functional training for stability

Effects of Grouped versus Alternating Functional Training on Shoulder Girdle and Lumbar-pelvic Girdle Stability: A Randomized Controlled Trial

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35 **Effects of Grouped versus Alternating Functional Training on Shoulder Girdle and**
36 **Lumbar-pelvic Girdle Stability: A Randomized Controlled Trial**

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38 Objective: We verified the effect of 10 weeks of structured FT grouped by muscular actions
39 (GFT) or alternating actions (AFT) on scapular and lumbar-pelvic girdle stability. Method:
40 One hundred and twenty adults (60 men; 60 women) were allocated into three groups, GFT (n
41 = 40) that performed the actions in sequence (squat - squat - pull - pull), AFT (n = 40) that
42 performed alternate actions (squat - pull - squat - pull) and the control group (CG, n = 40). The
43 shoulder girdle and pelvic girdle stability was assessed using the Octobalance Upper Body
44 Test. Results: The GFT increased stability after the intervention and compared to the CG (p =
45 0.003) as assessed by the relative range of the right (ES: 0.53) and left (ES: 0.57) hemispheres.
46 Besides, most results were within the instrument's error value and the magnitude of the effect
47 was moderate to trivial among the experimental groups. Conclusions: Therefore, ten weeks of
48 functional training performed in a grouped sequence promoted improvements in scapular and
49 lumbar-pelvic girdle stability.

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51 Keyword: Knee Osteoarthritis, Balance Test, Reproducibility.

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60 INTRODUCTION

61 The lumbar-pelvic-hip complex consists of musculoskeletal and ligamentous structures that
62 stabilize the spine and pelvis (Chang et al., 2017). Moreover, weaknesses and imbalances in
63 the musculoskeletal structures affect pelvic function, as well as the function of the shoulder
64 and adjacent structures (Pogetti et al., 2018; Radwan et al., 2014). Thus, exercises to improve
65 trunk stability and strength are considered essential in physical training, rehabilitation or injury
66 prevention programs (Andersson et al., 2017).

67 From this perspective, functional training (FT) is a strong alternative to increase strength and
68 trunk stability (Da Silva-Grigoletto et al., 2019; Shahtahmassebi et al., 2019), together with
69 improving performance and reducing the incidence of injuries (Distefano et al., 2013; Mesquita
70 et al., 2019). This method is based on multi-component exercises (agility, balance, endurance,
71 strength and muscle power) integrated in the same training session requiring intense activation
72 of trunk stabilizing muscles in tasks similar to activities of daily living, work and sport (Da
73 Silva-Grigoletto et al., 2020; La Scala Teixeira et al., 2017).

74 The sequence of exercises for FT can be grouped by muscle actions with exercises that refer
75 to the same functional action in sequence (e.g., squat followed by squat) or alternating, with
76 the functional actions being alternated during the circuit (e.g., squat followed by pushing). The
77 impact of the sequence of FT exercises has not been previously explored.

78 Impairments in the interaction or integration of trunk, pelvic and scapular muscular
79 coordination can affect functional performance (Tarnanen et al., 2012; Vega Toro et al., 2016).

80 Functional training is a possible strategy to enhance the coordination between trunk, scapular
81 and pelvic girdle in daily actions (Becker et al., 2018). Despite the numerous investigations
82 demonstrating the effectiveness of FT in improving performance in daily activities (De
83 Resende-Neto et al., 2019), its effects on the stability of the shoulder girdle and lumbar-pelvic
84 girdle are still unclear.

85 Another point is the difficulty in assessing the interaction between the scapular, pelvic and
86 trunk actions due to the complex neuromuscular issues involved. The current tests subject the
87 individual to dynamic challenges for the trunk seeking to bring the tests closer to reality. In this
88 line, the Upper Body Test was validated recently with excellent reproducibility (Gonzalo-Skok
89 et al., 2015), in this test the subject remains in a position of three supports (Bird dog) and with
90 one hand moves the arm in different directions challenging the abdominal muscles and the
91 stability of the scapular and pelvic girdle during movements.

92 Therefore, we verified, through a new form of evaluation, the effects of functional training
93 either with a grouped or alternating sequence on scapular and pelvic girdle stability in untrained
94 young adults. It was hypothesized that the grouped sequence training would be more effective
95 than the alternating sequence for improving scapular and lumbar-pelvic girdle stability due to
96 increased muscle stress when we group an action (three same exercises consecutively).

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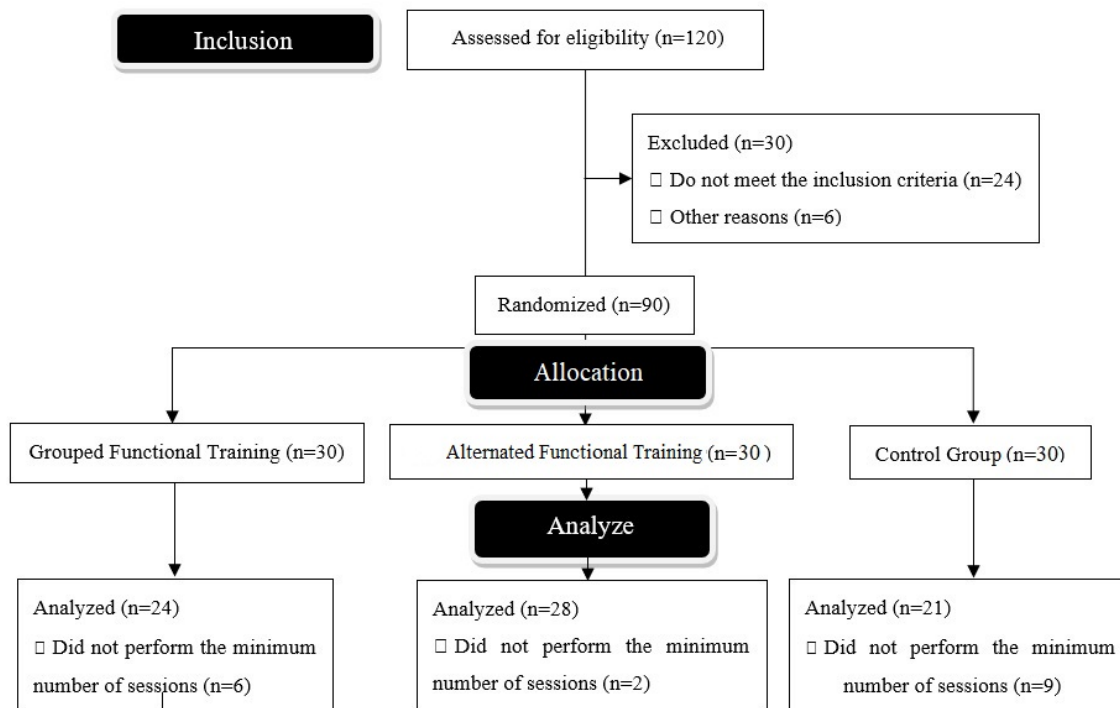
98 METHODS

99 This was a controlled and randomized trial, lasting 16 weeks. Weeks 1-2 and 15-16 were
100 designed to assess the stability of the shoulder girdle and lumbar-pelvic girdle, weeks 3-4 to
101 familiarize themselves with the exercise program and weeks 5-14 to apply the training protocol.
102 In addition, nutritional monitoring was carried out by recall to control one of the intervening
103 factors.

104 Participants

105 Based on a statistical power analysis (see statistical analysis section) 120 asymptomatic young
106 adults (60 men; 60 women) without restrictions for the practice of high intensity FT were
107 recruited through digital media and randomly allocated to three different groups, according to
108 their initial levels of stability, that's mean both groups there was the same among of individuals
109 stable and unstable. They were allocated to grouped functional training (GFT: $n = 40$; $23.8 \pm$

110 5.0 years), alternating functional training (AFT: $n = 40$; 25.9 ± 6.4 years and control group
 111 (CG: $n = 40$; 24.5 ± 5.14 years. Individuals without recent neurological, cardiac or orthopedic
 112 injuries (<1 year) were included and after the intervention, participants with low attendance
 113 (<85%) or who missed the assessment were removed from the analyses (figure 1).
 114



115

116 Figure 1. Flowchart.

117

118 The eligible individuals underwent an initial interview to record demographic, behavioral and
 119 health status. After clarifying the possible risks and benefits associated with the research,
 120 volunteers were asked to sign a Free and Informed Consent Form. This study followed the
 121 recommendations proposed by CONSORT (Schulz et al., 2010), was approved by the Research
 122 Ethics Committee of the Federal University of Sergipe (053820/2017) and is in accordance
 123 with the Declaration of Helsinki for research with humans.

124 Procedures

125 Participants completed 30 training sessions, lasting 60 minutes, three times a week and a
126 minimum recovery time of 48 hours between sessions. Each FT session was divided into four
127 blocks. In the first block of each session, the preparation of the movement was performed (10
128 min), with exercises for mobility of the main joints of the body, activation of the stabilizing
129 muscles of the trunk in addition to coordinating exercises. For core activation, ventral and
130 lateral plank exercises, bridge and bird dog exercise were used (Imai et al., 2014). Coordination
131 was stimulated with verbal commands or gestures guided by the instructors, in which the
132 subjects should perform actions of squatting, jumping and moving in the shortest possible time
133 (reaction time), in addition to gait exercises in the frontal and sagittal planes.

134 The main part of the session was divided into two major circuits (Neuromuscular I and
135 Neuromuscular II), each consisting of six exercises. In neuromuscular I (20 min), the exercises
136 were directed to the agility and muscle power of the lower and upper limbs, through exercises
137 with light or moderate loads performed at high speed of displacement, medicine ball pitches,
138 initially in the transversal plane, with progression to the front.

139 In neuromuscular II (25 min), the maximum dynamic force was stimulated through the
140 execution of the functional patterns of pushing, pulling, crouching, carrying and their
141 variations. They were used from exercises with body weight and variable resistance, such as
142 push-ups and the action of pushing with elastic bands of different densities and unilaterally.
143 The pull pattern varied between pull-ups (pulls) with the use of suspension straps initially in
144 vertical postures to horizontal positions and the use of elastic and free weights. Finally, the
145 crouching pattern used basic bilateral squats to unilateral executions and use of external loads
146 (Olympic bars, kettlebell).

147 Precisely in neuromuscular II, there was a methodological differentiation in the organization
148 or sequency of exercises in a grouped or alternated patterns by muscular actions. GFT carried
149 out the actions in the following sequence: crouch - crouch - pull - pull - push - push. On the

150 other hand, AFT performed the exercises alternately as follows: squat - pull - push - squat -
151 pull - push.

152 The fourth block, cardiometabolic (5 min), consisted of high intensity interval exercises (HIIT),
153 with equal effort and recovery time (density) between the groups, as well as the activities
154 developed (i.e., interval running).

155 The intensity of the main blocks was monitored and normalized between the groups using the
156 Borg effort scale (CR-10), in which the individuals mentioned a score referring to the degree
157 of effort (Arney et al., 2019). The scale was applied after each of the four training blocks. An
158 intensity ranging from 6 to 9 for training was established for all training sessions. The effort /
159 recovery ratio (exercise execution time and recovery), used in the last three blocks mentioned
160 above, was initially 30 s / 30 s (1-3 weeks), 40 s / 20 s (4-7 weeks), 45 s / 15 s (8-10 week).

161 The tests were performed pre- (week 0) and post-intervention (week 10) in the afternoon. The
162 measurements were taken by researchers blinded in relation to the exercise protocol, always
163 adjusting the devices and instructing the individuals in the execution of the tasks. All
164 individuals wore sportswear and were verbally encouraged during the assessments.

165 The measurements of body mass and height were performed using an anthropometric scale and
166 a stadiometer (Welmy, R-110, São Paulo, SP, Brazil), respectively. In addition, the body mass
167 index (BMI) was calculated using the weight divided by the height squared.

168 Upper Body Test: This test evaluated the stability of the scapular and lumbar-pelvic girdles
169 using OctoBalance® (Check Your Motion®, Basic Model, Albacete, Spain). Octobalance is a
170 validated instrument with good reproducibility (0.87 to 0.94) with values from 4.4 to 4.6 for
171 detecting minimal changes in the evaluation standards and 3.3 to 3.8 the side of the body
172 (reaching of the shoulder to the upper and lower body regions). The values obtained were
173 expressed in values relative (%) to the length of the upper limb (Fontes et al., 2020).

174 For evaluation, the length of the upper limbs of the subject in an upright posture was measured
175 from the acromion to the radio's styloid process. For this measurement, the shoulder was flexed
176 at 90°, with the elbow maintained in extension and the wrist in hyperextension (Gorman et al.,
177 2012). Three tests were performed followed by three more measures to measure the distances
178 obtained in each movement pattern of the Upper Body Test. An interval of 30 s was provided
179 between each measurement based on the procedures suggested by Gonzalo-Skok et al. (2015).
180 Two movement patterns were used for each body hemisphere, supralateral and inferolateral
181 (figure 2). The test began with the participant on their hands and knees. Their hands rested on
182 the OctoBalance® fixed platform on the side indicator arrows, knees on a thin layer of foam
183 with 90° flexion for the hips, knees, ankles and shoulders (Figure 2A). To assess the left
184 supralateral pattern, a hip and knee extension on the left side was requested, followed by
185 movement of the right upper limb, as shown in figure 2B. Then, the initial position was resumed
186 and the evaluation for the left inferolateral pattern was performed, again with hip and knee
187 extension movement of the mobile platform by the right upper limb obliquely across the body
188 as shown in figure 2C. After evaluating the left side, a contralateral evaluation was performed.
189



190

191 Figure 2. Upper Body Test assessment positioning: A. Initial position; B. Final position of the
192 left medial superior pattern; C. Final position of the left lateral inferior pattern.

193

194 All participants were instructed to maintain posture at the time of assessment, thus avoiding
195 trunk rotation, flexion of the lower limb in elevation, partial uncoupling of the shoulder joint
196 and flexion of the elbow for the supporting limb. Additionally, the participants were instructed

197 to maintain voluntary activation of the abdominal muscles, to ensure the position of the trunk,
198 and to breathe normally.

199 The test trial was invalidated and repeated for a maximum of three times in the following
200 situations: a) pushing the mobile platform sharply; b) move the mobile platform intermittently;
201 c) lose balance during the test movement or failing to return to the initial support; d) Do not
202 move the platform obliquely in line; e) exaggerated elbow flexion (approximately 15°) occurs
203 in the supporting member; f) losing hip extension; or g) to raise the lower limb ipsilateral to
204 the side that displaces the mobile platform (Fontes et al., 2020). The Upper Body Test index
205 for each pattern was obtained by using the arithmetic mean of the values obtained in each
206 direction and pattern, divided by the length of the limb corresponding to each side, and then
207 multiplied by 100.

208 Statistical analysis

209 The data were treated and analyzed using the Statistical Package for the Social Sciences (SPSS
210 - version 22) software. The sample calculation was performed based on the results of Fontes
211 et al. (2020), using G*power version 3.1.9.2 (Faul et al., 2007), requiring a sample of 23
212 individuals per group to obtain 80% statistical power. Assuming a sample loss during the
213 intervention, an additional 30% was added in an attempt to ensure sufficient statistical power.

214 The distribution of the data was verified using the Kolmogorov-Smirnov test, while the
215 homogeneity of the variances was assessed by the Levene test. Inferential analyses were
216 performed using a 2-way ANOVA (3x2) for repeated measurements, followed by the
217 Bonferroni post-hoc test to assess the interaction between the three group and time (pre- and
218 post-intervention) factors.

219 The effect size (ES) was analyzed to determine the magnitude of the effect independent of
220 sample size; ES was estimated by the difference from the standardized mean ($ES = (\text{Post mean} - \text{Pre mean}) / \text{Standard deviation pre}$) and classification proposed by Cohen (1988).

222 Classifications were interpreted based on the following criteria: <0.2 trivial effect; 0.2–0.49
 223 small effect; 0.50–0.8 moderate effect; and >0.8 large effect. For all analyzes, the statistical
 224 significance adopted was $p < 0.05$.

225

226 RESULTS

227 The general characteristics of the participants at the beginning of the study are shown in Table

228 1. No statistically significant main effect differences were found between the groups.

229

230 Table 1. General characteristics of participants in the (CG, $n = 21$) at the beginning of the
 231 intervention.

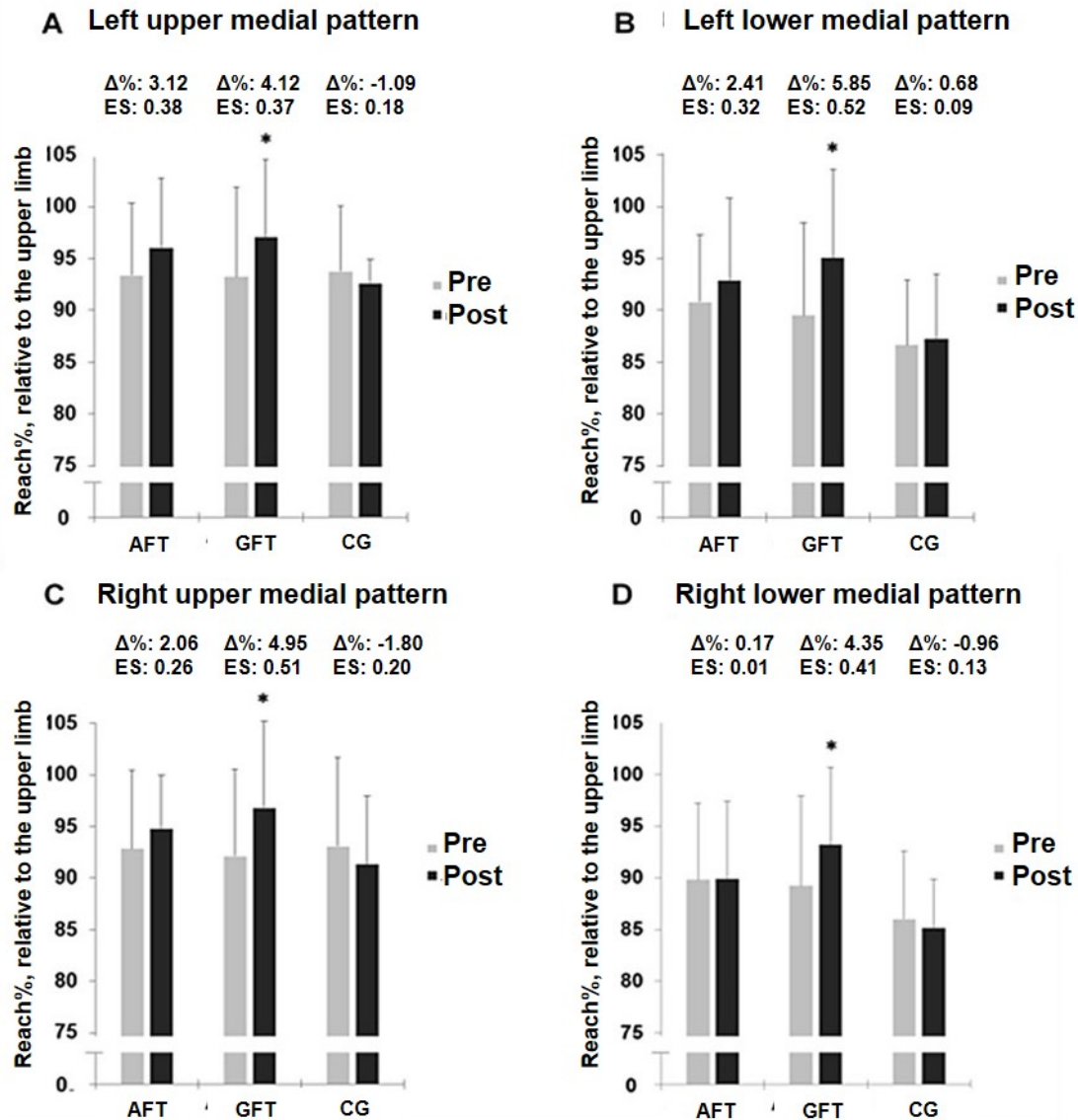
Characteristics	GFT (24)	AFT (28)	CG (21)	p
Age (years)	23.8 ± 5.0	25.9 ± 6.4	24.5 ± 5.14	0.31
Height (cm)	165.1 ± 7.2	164.74 ± 6.8	163.7 ± 8.7	0.88
Body mass (kg)	67.4 ± 9.8	68.2 ± 10.8	65.6 ± 9.8	0.30
BMI (kg/m ²)	24.65 ± 3.15	25.41 ± 3.82	23.99 ± 3.14	0.28

232 **Note.** BMI: body mass index; GFT: grouped functional training group; AFT: alternate functional
 233 training; CG: control group. Values presented as mean ± standard deviation.

234

235 A significant interaction demonstrated that only the GFT increased stability after the
 236 intervention and also when compared to the CG ($p = 0.003$) in the relative percentage range of
 237 the right and left hemispheres. In addition, most results showed to be within the instrument's
 238 error value and the magnitude of effect observed for the experimental groups ranged from
 239 moderate to trivial (figures 3 and 4).

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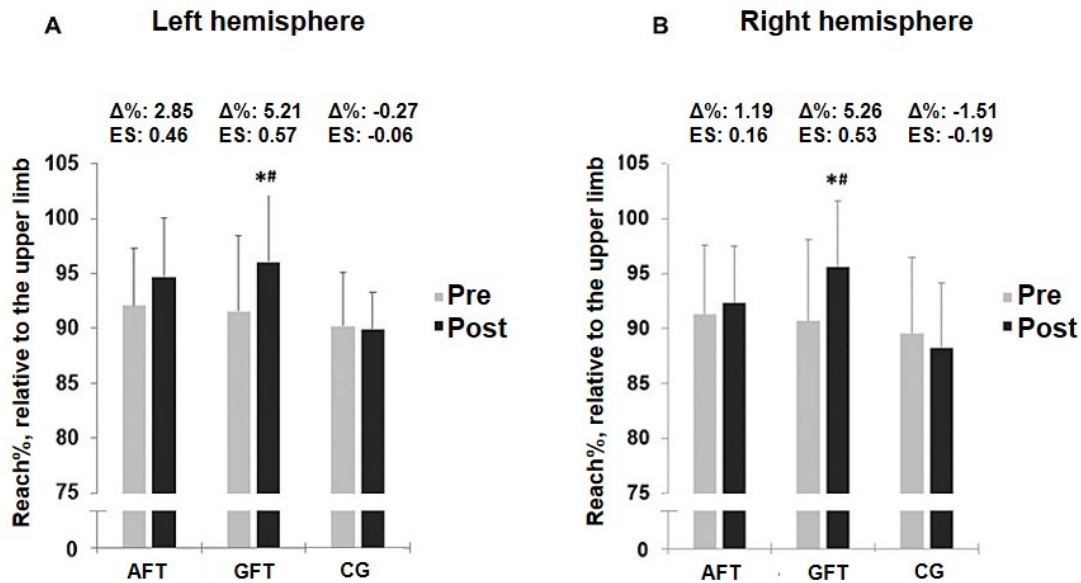


241

242 Figure 3. Effects of the groups on the percentage reach relative to the upper limb in the Upper

243 Body indices for each evaluated standard. Note. * $p < 0.05$ for intragroup comparison (pre

244 versus post).



245

246 Figure 4. Effects of the groups grouped functional training (GFT, n = 24), alternate training
 247 (AFT, n = 28) and control (CG, n = 21) on the percentage reach relative to the upper limb in
 248 the Upper Body indices for each body hemisphere. Note. * p <0.05 for intragroup comparison
 249 (pre versus post). ES = Effect Size; Δ = percentual change.

250

251 DISCUSSION

252 The main finding of this study is the improvement caused by GFT in the stabilization of the
 253 scapular and lumbar-pelvic girdle after 10 weeks of training, both in the right and left
 254 hemispheres. For all the evaluated patterns, low effect size and modifications between the pre-
 255 and post-test were obtained, which are within the error range of the evaluation instrument (4.4-
 256 4.6). This may be due to the low intensity of the training, however, it seems that the assessments
 257 of the both of side body are more sensitive to assess the stability of the shoulder girdle and
 258 pelvic girdle.

259 Thus, the improvement obtained by the GFT can be explained by the greater perceived exertion
 260 of training resulting from the consecutive execution of the same exercise, which can generate

261 greater metabolic acidosis and thus provide important adaptations in muscle resistance and
262 activation threshold of stabilizers (Brentano et al., 2017), confirming the initial hypothesis.

263 In relation to the effects of performing high-intensity exercises on functional test scores for the
264 upper limbs, Salo and Chaconas (2017), using the Y-Balance Test, observed a significant
265 reduction in the scores after a high intensity, fatigue-inducing, resistance training protocol for
266 upper limbs. However, this acute overload, if repeated over time, can generate a positive
267 adaptation for stabilization of the shoulder girdle and pelvic girdle that provides better scores
268 in the evaluation for the both side body (Marginson et al., 2005). In addition, the increase in
269 exercise exertion in the present study may have promoted changes in the tonic control of
270 synergistic structures so that the execution of the exercise is maintained over time (Brennecke
271 et al., 2009).

272 Furthermore, when exposed to high exertion (consecutive performance of the same exercise)
273 and consequently to greater fatigue, the lumbar muscles are capable of making changes in the
274 spatial distribution of muscle activity. These changes indicate relative adaptations in the
275 intensity of muscle contraction and can be attributed to the variation in the control of motor
276 units within a muscle and possibly between muscles (Farina et al., 2008). Asymptomatic
277 people show greater variability in muscle activation, suggesting that adequate motor variability
278 is necessary to optimize and maintain motor performance in dynamic actions and this plays an
279 essential role in the distribution of mechanical loads along the spine and consequently to delay
280 the fatigue.

281 In addition, during segmental movements performed on a daily basis, such as the movement of
282 sitting and getting up from a chair¹⁴, the reduced motor variability of trunk muscles is
283 associated with increased muscle fatigue and decreased resistance (Abboud et al., 2014; Roth
284 et al., 2019). Thus, we suggest that the GFT group was exposed to greater trunk fatigue and

285 this stress provided greater training of the motor variability of the trunk muscles, which
286 reflected in better performances in the Upper Body Test.

287 The slight difference in pelvic and scapular stabilization found in the GFT group, even in the
288 absence of specific exercises for trunk stabilization during training, can be partially explained
289 by the integrative multi-segmented characteristic with typical FT accelerations and
290 decelerations, providing a greater challenge to trunk stabilization. Such changes favor
291 improvement in motor control (Davin & Callaghan, 2016). As an example of functional
292 actions, when using the push pattern, during push-up exercises, the recruitment of the various
293 muscles of the trunk, shoulder and arms occurs in an integrated and simultaneous manner with
294 the aim of controlling movement (Marcolin et al., 2015). In addition, the use of suspension
295 exercises with instability (i.e., suspension bands) provides greater activity for the trunk or core
296 muscles, in an attempt to counterbalance uncoordinated movements, promoted by the
297 instability of the support base (Cugliari & Boccia, 2017; Escamilla et al., 2010).

298 The elevation of the contralateral upper and lower limb with the testing necessitates deep
299 stabilizers and scapular muscle activation (Pirouzi et al., 2013). The stabilization of the lumbar-
300 pelvic region is also important, due to the asymmetric positioning of the support base during
301 the Upper Body Test. There is an asymmetric abdominal muscle activation, so that there is an
302 increase in spine stiffness (Okubo et al., 2010). Thus, the stability in the test position is
303 explained by the mechanism of the anti-rotational action exerted by the oblique muscles, in
304 which there was a high muscle activity of the contralateral internal oblique and of the ipsilateral
305 external oblique, in relation to the upper limb in support at the base. In this sense, Okubo et al.
306 (2010) verified by means of electromyography that there is an ideal cooperation between the
307 activation of the oblique muscles (contralateral internal oblique and the ipsilateral external
308 oblique) to maintain the neutral posture of the pelvis and spine, when balancing the internal

309 and lateral forces of shear that are imposed on the spine and promote the reduction of forces
310 that are attributed to the spine.

311 In addition to this process of muscular cooperation, Vera-García et al. (2015) described trunk
312 stabilization as a multifactorial process that results from the interaction between sensory, motor
313 and neural systems, to maintain coordination of movements and maintenance of posture. This
314 interaction is also necessary to ensure when the stabilizing muscles will contract for the
315 production and transfer of forces to stabilize the body segments when performing functional
316 tasks³⁴. This concept can be called the timing's core. Thus, the assessment of the ability to
317 stabilize the scapular and lumbar-pelvic girdles in this study was carried out using the Upper
318 Body Test, showing the interaction between the core's timing and the movement of the upper
319 and lower limbs in a stable manner.

320 In this perspective, to our best knowledge, this is the first study that analyzed the effects of the
321 methodological organization of functional exercises on scapular and lumbar-pelvic girdle
322 stability. This fact makes it difficult to compare the results found with the current literature.
323 From the labor point of view, after 10 weeks, the supervised and organized FT in a grouped
324 manner promoted a succinct improvement in the scapular and lumbopelvic stability in active
325 young adults. Thus, it seems that grouping exercises for the same muscle function in a training
326 program can provide increased intensity that lead to long-term stability of the shoulder girdle
327 and pelvic lumbar.

328 Some limitations of the present study must be considered. The first of them, regarding the lack
329 of control for individuals' physical activities beyond the training period, which can be different
330 between the subjects and thus influence the magnitude of adaptations to training. However, this
331 aspect increases the external validity of the intervention. Another point was the lack of
332 quantification of the training volume, which makes our conclusions difficult. However, there
333 was a desired repetition range during the 10 weeks of intervention (8 and 12 repetitions per

334 exercise). Thus, further studies with longer intervention periods are needed to verify changes
335 in the physical adaptations of young adults to map possible deficits for stabilization of the
336 scapular and lumbar-pelvic girdle and thus prescribe interventions focused on training or
337 rehabilitation of these circumstances.

338

339 CONCLUSIONS

340 It is reproducible to perform the Lower Body Test with the Octobalance® platform for
341 the evaluation of the dynamic balance of lower limbs in women with knee osteoarthritis.

342 It was also possible to identify values of minimum detectable difference, values to be used as
343 a form of prognosis and improvement of these individuals.

344

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